

# A Mass-Conserving Toy Model of Blood Pulses in Arterial Networks

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January 22, 2021

# Presentation Overview

- 1 Statement of model PDE and physical motivation
- 2 Adapting the model PDE to a network
- 3 Local well-posedness of network model
- 4 Energy method for global well-posedness of network model
- 5 Some numerical experiments

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# Model setup

We study blood flow in a viscoelastic artery that is perfectly cylindrical in equilibrium

- $x$  = axial displacement along artery (artery is very long so  $x \in \mathbb{R}$ )
- $t$  = time
- $u(x, t)$  = deviation from equilibrium of artery's cross-sectional area
- Real parameters:  $\mu, \alpha, \nu, \geq 0$ ,  $\gamma \in [0, 1]$ , and  $p \in \mathbb{N}$

We suppose  $u$  solves the PDE

$$(1 - \mu^2 \partial_{xx}) u_t + \partial_x \left( \alpha u + \frac{\gamma}{p+1} u^{p+1} \right) - \nu u_{xx} = 0$$

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# Why gBBMB?

- Benjamin et al. 1972: original Benjamin-Bona-Mahony eqn. (BBM) analyzed, stressed as a more realistic substitute for Korteweg-de Vries eqn. (KdV)
- BBM is second-order in space (vs. third order KdV) and features short linear waves w/ bounded group velocity
- Erbay et al. 1992: generalized KdV-Burgers eqn. models blood vessel motion even when the artery walls are nonlinearly elastic
- I have taken Erbay et al.'s model and replaced KdV dispersion with BBM dispersion in light of the first two points
- Nonlinear dispersive models should work best in very long arteries, particularly the femoral artery

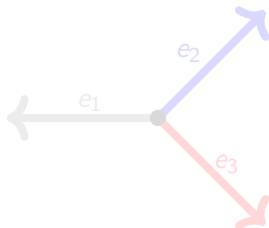
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# Flow in a Network of Arteries

**Question:** How do bifurcations of arteries or changes in artery elasticity (due to arteriosclerosis or stents) affect pulsatile blood flow?

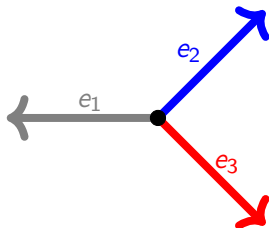
- To address question, we formulate our model on a **network**, a set of finitely many intervals glued together at various junctions
- Coefficients of model PDE are allowed to vary from edge to edge to reflect changes in artery elasticity
- Need to specify compatibility conditions at junctions



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# Stents in the Femoral Artery

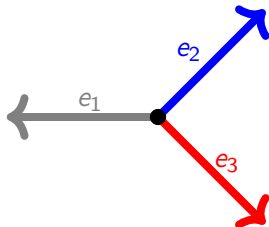
- As recently as 2017, use of stents in upper portion of femoral artery remains contentious (see for instance TASC II 2007 vascular surgery advisory vs. Goueffic et al. 2017)
- Mathematical modelling may be useful to determine best practices
- gBBMB is much too simple to give definitive answers, but may be a good toy model for basic wave-stent (or wave-sclerosis) interactions
- Predictions made w/ gBBMB should be benchmarked against simulations of the primitive equations to discover when gBBMB is a good enough substitute over long length scales (not addressed by me)

# Comparison with Related Work

- BBM has been studied on networks previously, most notably by Bona and Cascaval (B & C) in 2008
- B & C formulation does not guarantee conservation of total mass of blood in general, though my formulation takes care of this
- My proof of local well-posedness is a fixed-point argument identical to B & C, but I provide an explicit proof of global well-posedness by energy methods as well. I believe the explicit energy equation is really worth looking at.

# Model Setup 1

- Network  $X$  consists of  $N$  edges  $e_i$
- One incoming edge  $e_1 = (-\infty, 0]$ , from which a signal arrives at a central **junction** (the point  $x = 0$ ) and scatters off into the other edges, which are all copies of  $[0, \infty)$



## Model Setup 2

- Solution to gBBMB on network  $X$ : an array of  $N$  functions  $u_i(x, t)$ , with  $u_i$  satisfying gBBMB on the edge  $e_i$
- **Issue:** each  $u_i(x, t)$  needs to be assigned a boundary value at  $x = 0$  to have a hope of well-posedness... thus since we have  $i = 1, \dots, N$  we need to impose  $N$  conditions at the junction.

### Continuity Condition

For all  $i, j = 1, \dots, N$  and all  $t$ , we have  $u_i(0, t) = u_j(0, t)$ .

- Continuity only provides  $N - 1$  independent conditions. Need one more!



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## Model Setup 3

- Coeffs. of PDE now vary with  $i$ , so we write them as  $\mu_i, \alpha_i, \nu_i \geq 0, \gamma_i \in [0, 1]$

- Denote **advective flux** on the edge  $e_i$  by

$$f_i(u_i) = \alpha_i u_i + \frac{\gamma_i}{p+1} u_i^{p+1}$$

- Define the **total flux** on the edge  $e_i$  by

$$F_i(u_i) = -\mu_i^2 u_{i,xt} + f_i(u_i) - \nu_i u_{i,x}$$

- gBBMB on  $e_i$  can now be written in conservative form as

$$u_{i,t} + \partial_x (F_i(u_i)) = 0$$

## Model Setup 4

- Physically,  $M = \sum_i \int_{e_i} u_i$  represents the total “normalized” volume of blood in the arterial network  $X$ ... can also take this as total mass of blood assuming blood has unit mass density
- As anyone who has squished a water balloon knows,  $\frac{dM}{dt} = 0$  (mass must be conserved)!
- A quick check with the conservative form of gBBMB shows that mass is conserved provided we impose the following final junction condition:

### Mass Conservation Condition

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# Model Setup: Summary

$X$  a network with edges  $e_i$  ( $i = 1, \dots, N$ ), then we seek functions  $u_i(x, t)$  defined for  $(x, t) \in e_i \times [0, \infty)$  (with suitable regularity) satisfying the system

$$0 = (1 - \mu_i^2 \partial_x^2) u_{i,t} + \partial_x \left( \alpha_i u_i + \frac{\gamma_i}{p+1} u_i^{p+1} \right) - \nu_i u_{i,xx}$$

- +  $u_i|_{x=0} = u_j|_{x=0} \quad \forall i, j$  (continuity at junction)
- +  $F_{\text{in}}(u_{\text{in}})|_{x=0} = \sum [F_{\text{out}}(u_{\text{out}})]_{x=0}$  (mass conservation at junction)
- + initial conditions.

# Local Well-Posedness Preamble

- Now that we have a physically sensible model, must establish local-in-time well-posedness (LWP) of this model (existence and uniqueness of solutions, cts. dependence on initial data).
- Start by reviewing how to write gBBMB on a half-line  $[0, \infty)$  as a fixed-point problem
- Then, use the above together w/ junction conditions to write gBBMB on a network as a fixed-point problem (requires us to define function spaces on our network)

# Some Function Spaces

- $C_b^k(U)$  = real-valued functions on  $U \subseteq \mathbb{R}^n$  whose derivatives up to order  $k$  are cts. and bounded; this becomes a Banach space when endowed with sup-norm
- Given any Banach space  $A$ ,  $C_b(0, T; A)$  denotes the Banach space of all continuous functions  $u: [0, T] \rightarrow A$  equipped with the norm

$$\|u\|_{C_b(0, T; A)} = \sup_{[0, T]} \|u(t)\|_A. \quad (0.1)$$

- Also need less common fnc. spaces:

## Half-Line gBBMB Phase Space

$$\mathcal{B}_T^{k, \ell} \doteq \left\{ u \mid \forall i \in [0, k], j \in [0, \ell], \partial_t^i \partial_x^j u \in C_b([0, \infty) \times [0, T]) \right\}$$

# gBBMB on a Half-Line

- Given  $h(t) \in C_b[0, \infty)$ ,  $\varphi(x) \in C_b[0, \infty)$ , find  $T > 0$  and  $u(x, t) \in \mathcal{B}_T^{1,2}$  such that

$$\begin{aligned}(1 - \mu^2 \partial_x^2) u_t + (f(u))_x - \nu u_{xx} &= 0 \quad \forall (x, t) \in (0, \infty) \times (0, T), \\ u(0, t) &= h(t) \quad \forall t \in [0, T), \\ u(x, 0) &= \varphi(x) \quad \forall x \in [0, T).\end{aligned}$$

- At least formally,

$$u_t = (1 - \mu^2 \partial_x^2)^{-1} [-(f(u))_x + \nu u_{xx}].$$

Treat the above expression as an ODE for  $u$

- Once we find an explicit expression for  $(1 - \mu^2 \partial_x^2)^{-1}$ , solve the ODE and determine a nonlinear operator for which  $u$  arises as a fixed point.



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# Inverting $1 - \mu^2 \partial_x^2$

Lemma (Green's Function for  $1 - \mu^2 \partial_x^2$ )

Let  $\delta(x - y)$  denote the Dirac distribution centred at  $y \in \mathbb{R}$ . The function

$$G(x, y) \doteq -\frac{1}{2\mu} \left( e^{-\frac{(x+y)}{\mu}} - e^{-\frac{|x-y|}{\mu}} \right) : [0, \infty)^2 \rightarrow \mathbb{R}$$

satisfies the PDE

$$(1 - \mu^2 \partial_x^2) G(x, y) = \delta(x - y) \quad \forall (x, y) \in (0, \infty)^2$$

in the sense of distributions, with  $G(0, y) = 0$  and  $\lim_{x \rightarrow \infty} G(x, y) = 0 \quad \forall y \in [0, \infty)$ .

Thus we have

$$(1 - \mu^2 \partial_x^2)^{-1} g(x) = \int_0^\infty G(x, y) g(y) dy.$$

# Fixed-Point form of gBBMB on Half-Line

- Define some auxiliary objects by

$$K(x, y) \doteq \frac{1}{2\mu^2} \left( e^{\frac{-(x+y)}{\mu}} + \operatorname{sgn}(x-y) e^{-\frac{|x-y|}{\mu}} \right),$$

$$\mathbb{B}_{\text{adv}}[u](x, t) \doteq \int_0^t \int_0^\infty e^{-\frac{\nu}{\mu^2}(t-s)} K(x, y) f(u(y, s)) dy ds,$$

$$\mathbb{B}_{\text{visc}}[u](x, t) \doteq \frac{\nu}{\mu^2} \int_0^t \int_0^\infty e^{-\frac{\nu}{\mu^2}(t-s)} G(x, y) u(y, s) dy ds,$$

Note that  $G(x, y), K(x, y)$  are rapidly decaying! Important later.

- Solve linear ODE, integrate by parts  $\Rightarrow$  fixed-pt. formulation of gBBMB now becomes

$$u(x, t) = e^{-\frac{\nu t}{\mu^2}} \varphi(x) + \left( h(t) - h(0) e^{-\frac{\nu t}{\mu^2}} \right) e^{-\frac{x}{\mu}} + \mathbb{B}_{\text{adv}}[u](x, t) + \mathbb{B}_{\text{visc}}[u](x, t).$$

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## Definition

$$C_b(X) \doteq \{(u_1, \dots, u_N) \in (C_b[0, \infty))^N \mid u_1(0) = \dots = u_N(0)\},$$
$$H^1(X) \doteq (H^1(0, \infty))^N \cap C_b(X).$$

$C_b(X)$  becomes a Banach space when equipped with the norm

$$\|u\|_{C_b(X)} \doteq \max_{i=1,2,3} \|u_i\|_{C_b[0,\infty)}.$$

Additionally,  $H^1(X)$  becomes a Hilbert space when equipped with the sum inner product.

# Cauchy Problem for gBBMB on a Network

- For some  $T > 0$  and a given  $\varphi \in C_b(X)$ , find

$$u \in C_b([0, T]; C_b(X))$$

such that if  $u_i \doteq u|_{e_i}$  then

$$\begin{aligned}(1 - \mu_i^2 \partial_x^2) u_{i,t} + (f_i(u_i))_x - \nu_i u_{i,xx} &= 0, \quad i = 1, \dots, N, \\ u_i(0, t) &= u_j(0, t),\end{aligned}$$

$$\begin{aligned}F_{\text{in}}(u_{\text{in}})|_{x=0} - \sum [F_{\text{out}}(u_{\text{out}})]_{x=0} &= 0, \\ u_i(x, 0) &= \varphi_i(x).\end{aligned}$$

## Proposition (LWP for Network Problem)

*Given  $\varphi \in C_b(X)$  with  $\varphi_i \in C_b^2[0, \infty)$  for each  $i$ , there exists  $T > 0$  and a unique  $u$  satisfying the above (classically). That is,  $u_i \in \mathcal{B}_T^{1,2}$  for all  $i$ . Additionally,  $u$  depends continuously on the initial data  $\varphi$ .*

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# Proof of LWP

- Using the same Green's function strategy applied to the half-line problem, we can write gBBMB on a network as a fixed point problem.
- After some calculation leveraging *both* junction conditions (see lecture notes),

$$u_i(x, t) = e^{-\frac{\nu_i t}{\mu_i^2}} \varphi_i(x) + \left( \Phi[u] + \varphi(0) \left( 1 - e^{-\frac{\nu_i t}{\mu_i^2}} \right) \right) e^{-\frac{x}{\mu_i}} \\ + \sigma_i \mathbb{B}_{\text{adv},i}[u_i](x, t) + \mathbb{B}_{\text{visc},i}[u_i](x, t).$$

where  $\Phi[u] + \varphi(0) = u_i(0, t) \quad \forall i$  and  $\sigma_i = \pm 1$  (arising from change of variables  $x \mapsto -x$  on  $e_1$ ).

- Showing that right-hand side of the above defines a contraction on a ball in  $C_b([0, T]; C_b(X))$  is straightforward since we use sup-norms and  $\Phi, \mathbb{B}_{\text{adv},i}, \mathbb{B}_{\text{visc},i}$  are all integral ops. w/ rapidly decaying kernels.



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# Proof of LWP (cont.)

- Contraction Mapping Thm.  $\Rightarrow$  fixed-pt. form of the problem has a solution in  $C_b(X)$ , unique in some ball in  $C_b([0, T]; C_b(X))$ .
- To show *unconditional uniqueness* (without imposing soln. lives in ball), use a bootstrap argument.
- The particular structure of  $\Phi, \mathbb{B}_{adv,i}, \mathbb{B}_{visc,i}$  as nested integrals with nice kernels shows that the fixed point has the claimed differentiability ie. it gives a classical solution to gBBMB on each edge
- Similarly, we can get continuous (actually Lipschitz) dependence on the initial data  $\varphi(x)$ , possibly by shrinking the existence time  $T$ . Proof is now done!

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# Energy Estimate

## Definition

The **energy**  $E$  of  $u: X \rightarrow \mathbb{R}$  is defined to be

$$\frac{1}{2} \|u\|_{H^1(X)}^2 = \frac{1}{2} \sum_i \int_0^\infty |u_i|^2 + \mu_i^2 |u_{i,x}|^2 dx.$$

(w/ change of vars. for  $u_1$  implicit).  $H^1(X) =$  functions in  $C_b(X)$  with finite energy.

## Proposition (Energy Estimate)

For a solution  $u(x, t)$  to gBBMB on  $X$ ,

$$\frac{dE}{dt} \leq -h^2(t) \left[ \sum_i \sigma_i \left( \frac{\alpha_i}{2} + \frac{\gamma_i}{(p+1)(p+2)} h^p(t) \right) \right]$$

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The equation for  $dE/dt$  gives us a lot of mileage in proving global well-posedness:

## Corollary (Global Well-Posedness of Network Problem)

*If*

$$\sum_{i=1}^N \sigma_i \alpha_i \geq 0, \quad \sum_{i=1}^N \sigma_i \gamma_i \geq 0$$

*and  $p$  is even, then the solution to gBBMB valid up to time  $T$  can be extended to a unique global-in-time solution  $u \in C_b([0, \infty); H^1(X))$ .*

*If  $\sum_i \sigma_i \gamma_i = 0$ , the demand of an even  $p$  can be relaxed.*

# Sketch of GWP Proof

- Using the energy estimate, we find that  $\frac{dE}{dt} \leq 0$  by hypothesis. So the  $H^1(X)$ -norm of a solution to gBBMB on  $X$  decreases over time.
- By the Sobolev embedding  $H^1(X) \hookrightarrow C_b(X)$ , have that  $C_b(X)$ -norm of a soln. also decreases over time.
- Thus LWP result can be iterated: if  $T$  is small existence time,  $u(x, T)$  can be used as “initial data” to get soln on  $[T, T + T']$ ,...
- Energy argument + junction conditions give uniqueness.  
Proof is complete.

# Discussion of GWP

Are these parameter restrictions interesting?

- $\alpha_i > 0$  is necessary for long linear waves to go towards  $+\infty$ , and  $\gamma_i \geq 0$  by hypothesis
- According to Erbay et al. 1992,  $p = 2$  may capture genuinely nonlinear behaviour in a wider variety of elastic materials compared to  $p = 1$
- Since we expect coeffs. will not change too much from edge to edge,  $\sum_{i=1}^N \sigma_i \alpha_i \geq 0$ ,  $\sum_{i=1}^N \sigma_i \gamma_i \geq 0$  seems reasonable
- In the  $N = 2$  case, get GWP if only  $\mu_i, \nu_i$  vary from edge to edge, which means only linear (visco)elasticity of arteries changes. This is fine for a toy model



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- Solitary wave solns. to gBBM (blood pulses) parameterized by speed  $c \in (\alpha, \infty)$  and initial peak location  $x_0$ :

$$u(x, t) = \left[ A(p, \mu, \alpha, c) \cosh \left( \frac{x - x_0 - ct}{W(p, \mu, \alpha, c)} \right) \right]^{-2/p}.$$

- Main purpose of simulations here is to investigate how incoming solitary waves scatter off the junction of a two-edge network. Linear scattering can be understood analytically
- Simulations based on a **finite difference scheme** of Eilbeck and McGuire developed for BBM (three-level implicit, second order) and operator splitting to accommodate dissipative term.

## Numerics Outline 2

- In most simulations, we increase linear elasticity  $\mu$  from edge to edge. Physically: solitary blood pulse is going from a less rigid artery segment to a more rigid segment (representing sclerosis)
- Later, also change viscoelastic coefficient  $\nu$  from edge to edge
- To measure performance, look at how well simulation conserves mass of the solution,

$$M(t) = \sum_i \int_{e_i} u(x, t).$$

Denote percent relative error in mass by

$$\delta M \doteq 100 \frac{|M(t) - M(0)|}{M(0)} \%.$$

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# $\nu = 0$ Solitary Wave Scattering 1: No Reflection

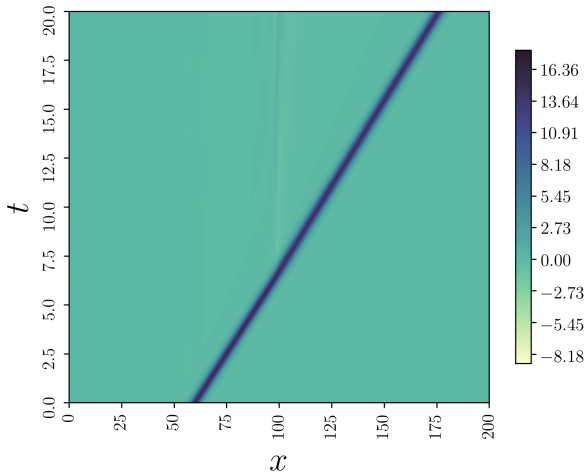


Figure:  $u(x, t)$  for a BBM solitary wave,  $\mu_2/\mu_1 = 1.1$ . Barely any change when moving across the interface ( $x = 100$ ).  $\delta M \leq 0.5\%$  here.

## $\nu = 0$ Solitary Wave Scattering 2: Reflection

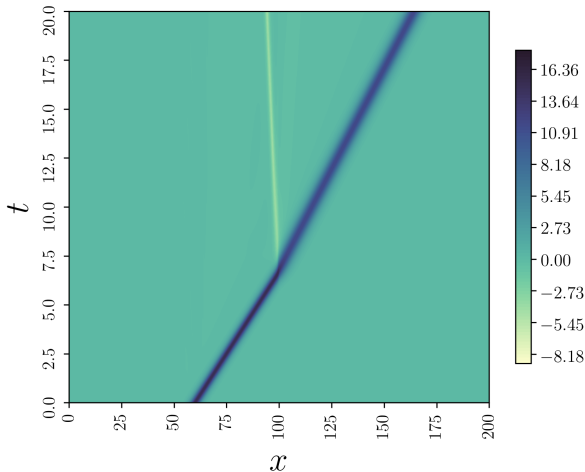


Figure:  $u(x, t)$  for a BBM solitary wave,  $\mu_2/\mu_1 = 1.5$ . Small, slow solitary wave reflected at interface ( $x = 100$ ). Transmitted solitary wave is slower and wider.  $\delta M \leq 0.5\%$  here.

# $\nu \neq 0$ Solitary Wave Scattering 1: $\mu_1 = \mu_2$

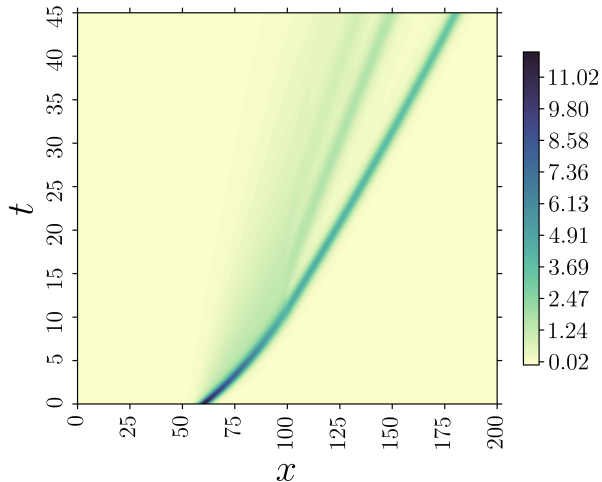


Figure:  $\mu_1 = \mu_2 = 1, \nu_1 = 1, \nu_2 = 0.1$ . Dissipative term creates a long “tail” in initial solitary wave. Wavemaker is generated at junction.  
 $\delta M \leq 0.13\%$  for this test.

## $\nu \neq 0$ Solitary Wave Scattering 2: $\mu_2/\mu_1 = 1.5$

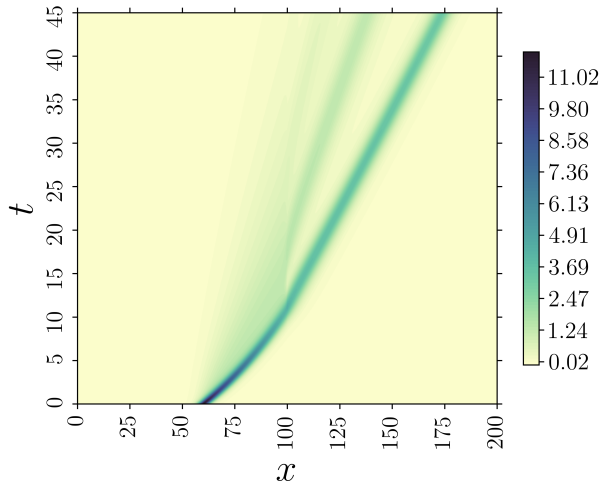


Figure:  $\mu_1 = 1, \mu_2 = 1.5, \nu_1 = 1, \nu_2 = 0.1$ . Only the speed of outgoing solitary waves changes from previous picture. Viscoelasticity has killed the reflected solitary wave.  $\delta M \leq 0.2\%$  for this test.



# Main Observations from Numerics (conjectures for analysis!)

- Speed of transmitted solitary wave changes across junction when  $\mu$  varies.
- Reflection of solitary waves is possible when  $\nu = 0$  and  $\mu_2/\mu_1$  is sufficiently large (further experiments not shown here actually imply reflection is also *amplitude*-dependent!)
- Sufficiently large jump in viscoelasticity can lead to wavemaker generated on outgoing edge.
- Strong viscoelasticity kills reflected solitary wave.
- More sophisticated numerical method is needed to efficiently handle multiple network edges and make behaviour at computational boundaries more physical. *Work in progress.*

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# Summary of Presentation

- Formulated gBBMB to guarantee mass conservation in full generality
- Proved local well-posedness, can often be extended to global
- Numerical simulations of nonlinear scattering with and without viscoelasticity lead to interesting questions

# Future Plans 1

- While reading up on BBM and gBBMB, I did not find a great deal of recent work on these eqns. In particular, long-time asymptotics has not been completely understood
- Estimates from the 80's and 90's (mainly from Albert, Souganidis & Strauss, and Dziubanski & Karch) on asymptotics of gBBM, gBBMB for  $p$  large enough
- $p$  can be made lower for gBBMB asymptotics, but dissipation swamps dispersion (see for instance Bona & Luo 2001)

**Question:** what do modern PDE/harmonic analysis tools have to tell us about the effects of dispersion on the long-time behaviour of gBBM? How large does  $p$  have to be?

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## Future Plans 2

Initial avenues of investigation: look at recent work on generalized KdV, since BBM is a substitute for KdV

- Harrop-Griffiths 2016: asymptotics for small solns of mKdV ( $u^2 u_x$  nonlinear term) without leveraging complete integrability. Primarily spatial methods (vector fields)
- Germain, Pusateri, & Rousset 2016: similar asymptotics, with applications to proving solitary wave stability. Primarily Fourier methods.

Hopefully the techniques in both these papers can allow us to take  $p \geq 2$  in gBBM. I have not yet seen good results for  $p$  this small. BUT, stationary phase techniques do not appear 100% useful for gBBM: big trouble! Stay tuned.

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